

TAT- μ Utrophin mitigates the pathophysiology of dystrophin and utrophin double-knockout mice

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Call JA, Ervasti JM, Lowe DA. TAT- μ Utrophin mitigates the pathophysiology of dystrophin and utrophin double-knockout mice. *J Appl Physiol* 111: 200–205, 2011. First published May 12, 2011; doi:10.1152/jappphysiol.00248.2011.—Previously, we demonstrated functional substitution of dystrophin by TAT- μ Utrophin (TAT- μ Utr) in dystrophin-deficient *mdx* mice. Herein, we addressed whether TAT- μ Utr could improve the phenotype of dystrophin and utrophin double-knockout (*mdx:utr*^{-/-}) mice. Specifically, we quantitatively compared survival and quality of life assessments in *mdx:utr*^{-/-} mice receiving TAT- μ Utr protein administration against placebo-treated *mdx:utr*^{-/-} mice (PBS). Additionally, skeletal muscles from TAT- μ Utr and PBS mice were tested in vivo and ex vivo for strength and susceptibility to eccentric contraction-induced injury. We found the TAT- μ Utr treatment extended life span 45% compared with mice administered PBS. This was attributed to significantly increased food consumption (3.1 vs. 1.8 g/24 h) due to improved ability to search for food as daily cage activities were greater in TAT- μ Utr mice (e.g., 364 vs. 201 m ambulation/24 h). The extensor digitorum longus muscles of TAT- μ Utr-treated double-knockout mice also displayed increased force-generating capacity ex vivo (8.3 vs. 6.4 N/cm²) and decreased susceptibility to injury ex vivo and in vivo. These data indicate that the functional benefits of TAT- μ Utr replacement treatment extend to the *mdx:utr*^{-/-} double-knockout mouse and support its development as a therapy to mitigate muscle weakness in patients with Duchenne muscular dystrophy.

plantarflexion torque; posterior crural muscles; Duchenne muscular dystrophy

DUCHENNE MUSCULAR DYSTROPHY (DMD) is a progressive muscle wasting disease caused by the loss of the protein dystrophin. Patients with DMD experience precipitous decrements in muscle function with age (23), resulting in wheelchair reliance for mobility by their early teens and ventilator respiratory assistance in their early twenties (18). Muscle function is compromised by the destabilization of the sarcolemma, a result of dystrophin deficiency (2), rendering skeletal muscle susceptible to contraction-induced injury (26). Without a cure, strategies to mitigate the disease progression and improve muscle function have been developed to compensate for dystrophin deficiency by boosting the presence of dystrophin-like cytoskeletal proteins (5, 15, 17, 25). Specifically, utrophin, a protein homologue of dystrophin, sufficiently compensates for dystrophin and improves the phenotype of *mdx* mice, the primary animal model for DMD (11, 28, 30, 33).

Previously, we reported on the efficacy of TAT- μ Utrophin (TAT- μ Utr) protein administration to boost in vivo levels of

utrophin in dystrophic skeletal muscles from *mdx* mice (29). TAT- μ Utr is biochemically stable in skeletal muscle and functionally substitutes for dystrophin forming a μ Utrophin-glycoprotein complex at the sarcolemma (29). Skeletal muscles from *mdx* mice that received TAT- μ Utr presented with a decrease in centrally nucleated fibers, an increase in muscle force, and a diminished susceptibility to contraction-induced injury, indicating TAT- μ Utr protein administration mitigates the dystrophic disease in *mdx* mice by reinforcing the sarcolemma. However, given the mild phenotype of the *mdx* mouse compared with patients with DMD, the more clinically relevant mouse model is the dystrophin and utrophin double-knockout mouse (*mdx:utr*^{-/-}; 8, 13).

Phenotypically, *mdx:utr*^{-/-} mice are described by a lack of mobility, abnormal gait, abnormal field behavior, joint contractures, severe weight loss, and a shortened life span compared with *mdx* mice (8, 13). Whereas *mdx* mice exhibit an ~25% reduction in skeletal muscle force compared with wild-type mice (22), *mdx:utr*^{-/-} mice exhibit a 60% reduction in peak force (13) and a 38% reduction in skeletal muscle force normalized to muscle cross-sectional area (15). The loss of muscle function in *mdx:utr*^{-/-} mice presumably would contribute to decrements in cage activity, increasing the difficulty to forage for food. Notably, *mdx:utr*^{-/-} mice given a mixture of powdered food and a dish of water on the cage floor were reported to have maintained their body mass for a longer period of time (8). Herein, we sought to determine whether TAT- μ Utr protein administration could attenuate these phenotypes in the *mdx:utr*^{-/-} mouse by improving skeletal muscle function.

MATERIALS AND METHODS

TAT- μ Utr. TAT- μ Utr protein was expressed and purified as previously described (29). Final protein concentrations varied between 4.5 and 9.2 mg/ml.

Mice and study design. The *mdx:utr*^{-/-} mice used in this study were established from *mdx:utr*^{+/-} breeder pairs obtained from Virginia Polytechnic Institute and State University (14) that descended from Washington University (13). Mice were bred and maintained in a specific pathogen-free environment. The genotype of each offspring was determined by PCR analysis of DNA isolated from tail snips as described in detail previously (14). Both male and female mice were used for this study. All mice were given commercial rodent chow and water ad libitum and were housed on a 12-h light/dark cycle. In addition to the food and water provided on cage tops, extra food was placed on the floor of each cage and moistened with water. Cages were changed weekly and moistened food was checked daily for the absence of mold. All protocols and animal care procedures were approved by the University of Minnesota Animal Care and Use Committee.

Two groups of *mdx:utr*^{-/-} mice were used for this study. *Group 1* consisted of 29 *mdx:utr*^{-/-} mice that were assessed only for life span survival. *Group 2* consisted of 22 *mdx:utr*^{-/-} mice used to assess

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quality of life (i.e., cage activity and food consumption) and in vivo and ex vivo muscle functions. Within each group, mice received twice weekly intraperitoneal injections of TAT- μ Utr at 8.5 μ g/g BM (TAT- μ Utr; $n = 14$) or equal volume injections of sterilized PBS ($n = 15$) starting at age 14 days (per Ref. 29). All mice were weaned from dams and into individual cages at age 21 days.

Survival. To address whether TAT- μ Utr improves the $mdx:utr^{-/-}$ mouse phenotype, we determined whether TAT- μ Utr prolonged the life span of $mdx:utr^{-/-}$ mice. Every morning the health of each mouse was determined by observation either by the primary investigator or a laboratory technician. Time of death was determined by the presence of a carcass on morning inspection or if during the day euthanasia was recommended by a veterinary doctor. The latter occurred twice, and both times mice were found recumbent with a slow heart rate and deep breaths occurring sporadically.

Cage activity assessment. At age 30 days, $mdx:utr^{-/-}$ mice were monitored for 24-h cage activities using activity chambers (Med Associates, St. Albans, VT). Infrared arrays in the x -, y -, and z -axes within the activity chambers created a three-dimensional space where cage activity could be monitored by beam breaks. Ambulatory distance was measured by beam breaks occurring in the x - and y -axis while vertical movements were counted by beam breaks occurring in the z -axis. Beam breaks occurring within a 2×2 -in. area subsequent to the ambulatory cessation for >20 s were counted as stereotypic movements. Direct observation of stereotypic movements can best be described as self-grooming. Active time was calculated by the amount of time during the 24 h that each mouse spent ambulating, jumping, rearing, and grooming.

In addition to monitoring cage activity, food consumption was also measured during the 24-h observational period. Pellets of food, ~ 6 – 7 g each, were placed on the floor of the activity cage. The following day the remaining pellet and small particles of food were collected and weighed to determine food consumption per 24 h.

In vivo functional measurements. The plantarflexor contractile performance of the posterior crural muscles (i.e., gastrocnemius, soleus, plantaris muscles) was measured in vivo for TAT- μ Utr and PBS mice. We chose to assess hindlimb plantarflexor muscles in vivo for strength and susceptibility to injury because the posterior crural muscles (i.e., gastrocnemius) are more active during ambulation compared with the anterior crural muscles (32). Mice were given a mixture of fentanyl citrate (10 mg/kg BM), droperidol (0.2 mg/kg BM), and diazepam (5 mg/kg BM) and left hindlimbs were shaved and antiseptically prepared by applications of betadine and ethanol. Each mouse was positioned on its right side on a 37°C heated platform with its left foot attached to a machined shoe located on the shaft of a servomotor (model 300B-LR; Aurora Scientific, Aurora, Ontario, Canada). Two platinum electrodes (model E2-12; Grass Technologies, West Warwick, RI) were inserted subcutaneously on either side of the sciatic nerve. To avoid recruitment of the anterior crural muscles responsible for dorsiflexion, the common peroneal nerve was severed. Peak isometric torque was optimized by varying the voltage delivered to the sciatic nerve by the stimulator and stimulus isolation unit (models S48 and SIU5, respectively; Grass Technologies). The parameters for stimulation were set at a 200-ms contraction duration consisting of 0.5-ms square-wave pulses at 150 Hz. Torque as a function of stimulation frequency was then measured during seven isometric contractions at varying stimulation frequencies (20, 40, 60, 80, 100, 125, 150 Hz). Next, the posterior crural muscles were injured by performing 20 eccentric contractions. Muscles were stimulated for 120 ms using the optimal voltage and 150 Hz (16). During stimulation, muscles were stretched from 19° of ankle plantarflexion to 19° of ankle dorsiflexion at an angular velocity of 2000°/s. Eccentric contractions were separated by 10–12 s, and the entire protocol lasted 3.5 min. The selection of a 20 eccentric-contraction protocol was based on preliminary data showing torque loss did not significantly worsen after 20 eccentric contractions. A 5-min rest followed the protocol before maximal isometric torque and torque as a function of stimu-

lation frequency were reassessed. The primary outcome measurements were pre- and post-injury maximal isometric torque and torque-frequency normalized to body mass ($N \cdot mm^{-1} \cdot kg \cdot BM^{-1}$) and torque loss during the eccentric contraction protocol [i.e., (*eccentric contraction #2* – *eccentric contraction #1*)/*eccentric contraction #1*]. Isometric and eccentric torques reported herein are indicative of the peak isometric and eccentric torques generated during the respective contractions.

Ex vivo contractility. EDL muscles from TAT- μ Utr and PBS mice were analyzed ex vivo for force-generating capacities. We chose to assess the hindlimb dorsiflexor EDL muscle ex vivo for contractility and susceptibility to injury for consistency between this and our previous work (29). Mice were anesthetized with pentobarbital sodium (25 mg/kg BM) and muscles were mounted to a dual-mode muscle lever system (300B-LR; Aurora Scientific) and incubated at 25°C in an oxygenated bath as previously described (1, 6, 36). Muscles were maintained at a 0.4 g resting tension (L_0) throughout the experiment (as per 34, 35). Following a 10-min quiescent period, muscles underwent a single passive stretch to 1.05 L_0 . Peak twitch force was elicited with a 0.5-ms pulse at 150 V. Maximal isometric tetanic force (P_0) was performed at 150 V and at 180 Hz for 400 ms (Grass S48 stimulator delivered through a SIU5D stimulus isolation unit; Grass Telefactor, Grass Technologies). Active stiffness was determined by applying a sinusoidal length oscillation of 0.01% L_0 at 500 Hz at peak force of a single tetanic isometric contraction (12, 31). One minute later, an injury protocol consisting of five eccentric contractions was performed, as per previous work in $mdx:utr^{-/-}$ (9, 14) mice and our previous work in mdx mice (1, 29). Specifically, muscle were passively shortened to 95% L_0 and stimulated for 133 ms while the muscle was simultaneously lengthened to 105% L_0 at 0.75 L_0 /s, and then passively returned to L_0 . Each eccentric contraction was separated by 3 min of rest to avoid fatigue (9, 14, 21). Three minutes after the last eccentric contraction, a final isometric tetanic contraction was performed. Muscle cross-section area was calculated as previously described (3, 34) giving consideration to muscle mass, length, pennation, and density. Maximal isometric and eccentric forces were recorded as the peak isometric and eccentric forces generated during each contraction, respectively. Specific forces (sP_0) were calculated by dividing P_0 by muscle cross-sectional area. Eccentric contraction-induced injury was determined by eccentric force loss during the course of the injury protocol [(*contraction #5* – *contraction #1*)/*contraction #1*] and also by the decrement in maximal isometric tetanic force [(*postP*₀ – *P*₀)/*P*₀].

Muscle mass. Following ex vivo preparations all mice were killed and the tibialis anterior, gastrocnemius, and heart along with extensor digitorum longus muscles, were snap frozen in liquid nitrogen and stored at -80°C . Masses for frozen muscle were later recorded using a microbalance (Sartorius CPA225D; Mettler Toledo, Boston, MA).

Statistics. Survival proportions between TAT- μ Utr and PBS mice were statistically analyzed using both Log-Rank and Wilcoxon tests. A Student's t -test was used to detect differences between groups concerning cage activities, food consumption, in vivo torque, ex vivo contractility characteristics, and torque and force loss percentages following eccentric contraction-induced injury in vivo and ex vivo, respectively. Data are reported as means \pm SE.

RESULTS

The first group of $mdx:utr^{-/-}$ mice were injected twice weekly with TAT- μ Utr or sterilized PBS. The life span of $mdx:utr^{-/-}$ mice receiving injections of TAT- μ Utr was 45% longer than mice receiving sterilized PBS (median life span: 43.5 ± 2.0 vs. 30.0 ± 1.8 days, respectively; $P < 0.001$; Fig. 1A). Maximal life span was also increased for TAT- μ Utr mice (64 vs. 50 days, respectively; $P < 0.001$). Body masses recorded twice weekly during injection showed no significant

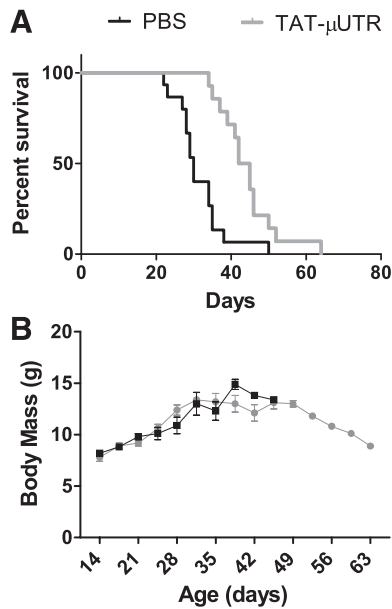


Fig. 1. Effect of TAT- μ Utr on survival. A: Kaplan-Meier curves. Black bar, PBS, $n = 15$; gray bar, TAT- μ Utr, $n = 14$. Survival proportions were extended by ~ 2 wk with TAT- μ Utr treatment; however, treatment did not affect body mass during this time (B).

difference between the two groups ($P = 0.517$, Fig. 1B). Masses of hindlimb muscles and hearts from TAT- μ Utr and PBS mice were analyzed to determine if TAT- μ Utr affected muscle size. There were no differences in tibialis anterior, gastrocnemius, EDL, or heart muscle masses between TAT- μ Utr and PBS mice for absolute muscle masses ($P \geq 0.280$) or muscle masses normalized to body mass ($P \geq 0.222$).

To investigate factors that may have contributed to an extended life span with TAT- μ Utr, we used a second group of *mdx:utr*^{-/-} mice to assess quality of life and muscle function both in vivo and ex vivo.

Quality of life, as measured by food consumption and cage activity, was assessed at age 30 days for both TAT- μ Utr and PBS mice. This age was chosen because it corresponded with the median life span of PBS-treated mice from the first group of *mdx:utr*^{-/-} mice.

At age 30 days there was no difference in body masses between TAT- μ Utr and PBS mice (12.0 ± 1.0 vs. 10.8 ± 1.0 , respectively; $P = 0.371$). However, during the 24-h activity observational period, TAT- μ Utr mice consumed 72% more food (3.1 ± 0.3 vs. 1.8 ± 0.2 g/24 h, respectively; $P = 0.002$). We attributed this to a greater ability to search for food because three parameters of cage activity were improved in TAT- μ Utr mice compared with PBS mice: ambulatory distance (364 ± 48 vs. 201 ± 22 m/24 h, respectively; $P = 0.004$); stereotypic counts (45.5 ± 2.6 vs. 36.6 ± 33 thousand counts/24 h, respectively; $P = 0.045$); active time (232 ± 18 vs. 178 ± 18 min/24 h, respectively; $P = 0.028$; Fig. 2A).

Correlation analyses were performed to determine if cage activities were associated with food consumption. Positive correlations existed between the amount of food consumed and ambulatory distance ($r = 0.5448$; $P = 0.024$), stereotypic activity ($r = 0.6612$; $P < 0.001$), and active time ($r = 0.5765$; $P = 0.015$; Fig. 2, B–D).

Maximal isometric in vivo torque was not different between TAT- μ Utr and PBS mice (360 ± 20 vs. 340 ± 15 N \cdot mm⁻¹·kg BM⁻¹, respectively; $P = 0.632$; Fig. 3A). Eccentric torque during the injury protocol was reduced $\sim 60\%$ from *eccentric contraction #1* to *eccentric contraction #20* in both groups ($P = 0.805$). TAT- μ Utr did affect isometric torque loss following the eccentric injury protocol as TAT- μ Utr mice produced 50% more torque compared with PBS mice (166 ± 19 vs. 111 ± 22 N \cdot mm⁻¹·kg BM⁻¹, respectively; $P = 0.047$; Fig. 3A). Isometric torques as a function of stimulation frequency pre- and post-injury are shown in Fig. 3B. Consistent with maximal isometric torque, torques elicited at stimulation frequencies 60–150

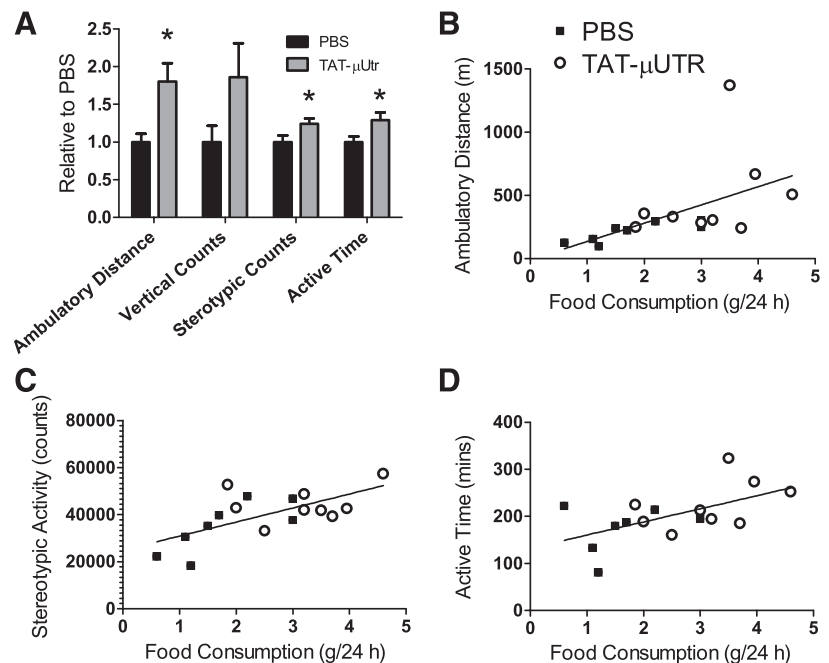


Fig. 2. Effect of TAT- μ Utr on cage activities. A: ambulatory distance, stereotypic movement, and active time were improved with TAT- μ Utr treatment as shown relative to PBS. Additionally, food consumption was positively correlated with ambulatory distance (B), stereotypic activity (C), and active time (D). * $>$ PBS; $P \leq 0.05$.

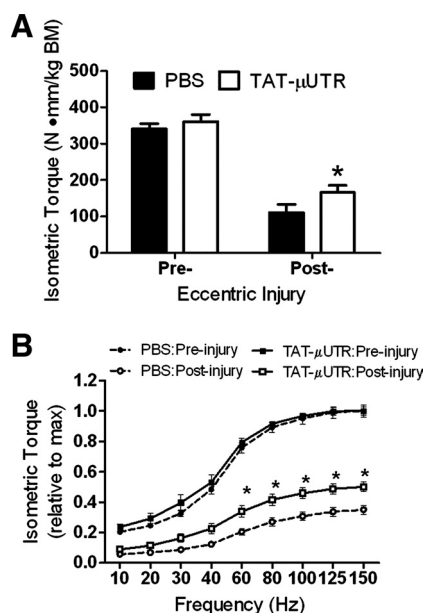


Fig. 3. Effect of TAT- μ Utr on in vivo muscle function. *A*: torque loss by the gastrocnemius-soleus-plantaris muscle group following eccentric injury was attenuated with TAT- μ Utr treatment. *B*: pre- and post-injury torque-frequency curves shown relative to maximal preinjury torque. * > PBS; $P \leq 0.05$.

Hz assessed postinjury were greater for TAT- μ Utr compared with PBS mice ($P \leq 0.032$). These data suggest that muscles from TAT- μ Utr-treated mice were less susceptible to eccentric contraction-induced injury.

To determine whether individual muscles from TAT- μ Utr-treated mice had better contractility or were less susceptible to eccentric contraction-induced injury, we tested EDL muscles *ex vivo*. There were no differences between groups in absolute twitch, tetanic, or eccentric forces generated by isolated EDL muscles (Table 1), although there were trends for peak isometric and eccentric forces to be greater in EDL muscle from TAT- μ Utr mice ($P = 0.068$ and $P = 0.080$, respectively). However, maximal isometric force normalized to muscle cross-sectional area (i.e., specific tetanic force) was 30%

Table 1. *Ex vivo* EDL muscle contractility for TAT- μ Utr and PBS mice

	PBS	TAT- μ Utr	<i>P</i> value
Mass, mg	3.2 \pm 0.4	3.7 \pm 0.4	0.448
Length, mm	9.2 \pm 0.3	9.7 \pm 0.4	0.379
CSA, mm ²	0.72 \pm 0.08	0.81 \pm 0.07	0.492
Twitch			
<i>P</i> ₀ , mN	17.8 \pm 2.2	22.9 \pm 3.2	0.205
TPT, ms	24.1 \pm 2.5	31.8 \pm 5.5	0.216
RT _{1/2} , ms	46.8 \pm 6.1	40.1 \pm 4.6	0.444
Tetanic			
<i>P</i> ₀ , mN	47.0 \pm 7.2	73.1 \pm 11.5	0.068
+d <i>P</i> /d <i>t</i> , N/s	1.8 \pm 0.3	2.4 \pm 0.3	0.220
-d <i>P</i> /d <i>t</i> , N/s	-1.0 \pm 0.3	-1.8 \pm 0.4	0.185
Peak eccentric force, mN	93.1 \pm 12.7	137.7 \pm 20.6	0.080
Passive stiffness, N/m	23.7 \pm 1.4	20.3 \pm 2.2	0.225
Active stiffness, N/m	179.5 \pm 16.0	223.3 \pm 21.0	0.136

Values expressed as means \pm SE. *P*₀, peak twitch force; TPT, time to peak twitch force; RT_{1/2}, one-half relaxation time; *P*₀, maximal isometric tetanic force; +d*P*/d*t*, maximal rate of tetanic force development; -d*P*/d*t*, maximal rate of relaxation.

greater in TAT- μ Utr mice compared with PBS mice (8.3 ± 1.0 vs. 6.4 ± 0.4 N/cm², respectively; $P = 0.026$; Fig. 4A). This is an ~15% relative recovery compared with the initial deficit between wild-type and *mdx:utr*^{-/-} mice [wild-type specific force (18.9 ± 1.0 N/cm²); data not shown]. Specific eccentric force was also 34% greater in TAT- μ Utr mice compared with PBS mice (17.0 ± 1.9 vs. 12.7 ± 0.6 N/cm², respectively; $P = 0.035$).

Twitch and tetanic force-time tracings were analyzed to determine whether TAT- μ Utr affected properties indicative of how fast the EDL muscle contracted and relaxed. There were no differences in these twitch and tetanic parameters between groups (Table 1). Both passive and active stiffness, which reflect the muscle's resistance to lengthening due to noncontractile elastic elements and myosin cross bridges that are strongly bound to actin, respectively, were also not significantly different between groups (Table 1).

There was no effect of TAT- μ Utr on EDL muscle force loss during the eccentric injury protocol ($P = 0.385$; Fig. 4B), but specific tetanic force following eccentric contraction-induced injury was significantly greater in TAT- μ Utr mice compared with PBS mice (4.1 ± 0.6 vs. 2.1 ± 0.3 N/cm², respectively; $P = 0.012$; Fig. 4A). These data complement the *in vivo* findings and reinforces that TAT- μ Utr mitigates susceptibility to contraction-induced injury.

DISCUSSION

Our results show that TAT- μ Utr ameliorated the *mdx:utr*^{-/-} mouse phenotype, most notably survival, by increasing skeletal muscle strength and improving activity and food consumption without any increase in body mass. We are not the first to report an improvement in the phenotype of *mdx:utr*^{-/-} mice

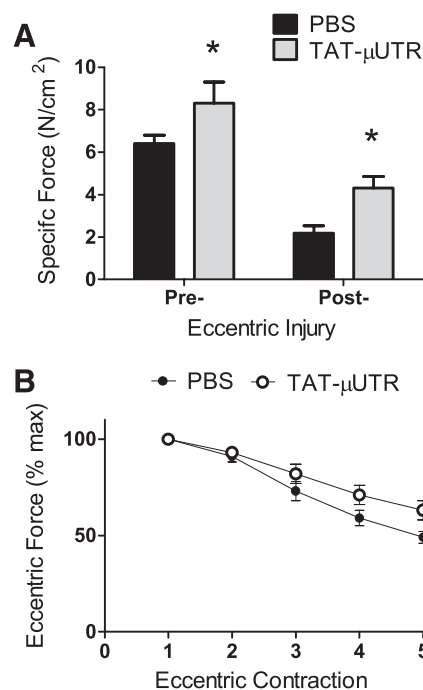


Fig. 4. Effect of TAT- μ Utr on *ex vivo* muscle contractility. *A*: TAT- μ Utr improved pre- and post-injury specific tetanic force. *B*: force loss during an eccentric injury protocol was not significantly affected by TAT- μ Utr. * > PBS, $P \leq 0.05$.

with μ Utrophin or full-length utrophin upregulation (24, 27); however, our findings establish the efficacy of direct protein delivery in improving *mdx:utr*^{-/-} mice. Here, TAT- μ Utr administration affected significant functional and quality of life improvements. We previously demonstrated that TAT- μ Utr administration had no effect on expression of full-length utrophin from the endogenous gene (29), suggesting it could be employed in conjunction with other treatment strategies to perhaps achieve additive efficacy.

We chose cage activity as an indication of quality of life and as a quantitative means to characterize the effects of TAT- μ Utr and PBS mice. Previously, we showed that wild-type mice were significantly more active than *mdx* mice in terms of ambulatory distance (700 vs. 450 m/24 h) and total active cage time (5.0 vs. 3.5 h/24 h), demonstrating the reliability of cage activity monitoring to quantitatively measure phenotypes (19). Here we detected that TAT- μ Utr mice spend 30% more time per day being active and achieved ambulatory distances 81% greater than PBS mice, which approaches ambulation achieved by *mdx* mice (364 vs. 450 m/24 h, TAT- μ Utr and *mdx*, respectively). Similar improvements in ambulation (i.e., voluntary wheel running) are observed with μ Utrophin upregulation via recombinant adeno-associated viral vectors (24). The increased ability to ambulate through an environment likely affords treated *mdx:utr*^{-/-} mice the opportunity to find and consume more food, as was shown in our study. The systems most likely affected by μ Utrophin therapy that could explain the subsequent increased activity are the skeletal muscle and cardiovascular systems.

Our investigation focused on the function of the posterior crural skeletal muscles in vivo and the EDL muscle ex vivo. To our knowledge we are the first to report in vivo plantarflexion torque capacity for the *mdx:utr*^{-/-} mouse. Maximal isometric torques are lower in *mdx:utr*^{-/-} mice compared with *mdx* and wild-type mice (340 vs. 450 and 670 N \cdot mm⁻¹·kg BM⁻¹, respectively, *mdx* and wild-type values are unpublished). Although preinjury torques were not improved with TAT- μ Utr, significantly improved postinjury torques suggest protection of the posterior crural muscles from eccentric contraction-induced injury. This finding was recapitulated ex vivo by greater postinjury EDL specific tetanic force in TAT- μ Utr-treated mice. Specific forces reported herein were low compared with previous reports, although EDL force-generating capacity is highly variable for the *mdx:utr*^{-/-} mouse model (8, 9, 14, 20, 22). Previously, *mdx* mice overexpressing full-length utrophin or injected with TAT- μ Utr exhibited marked improvements in EDL muscle force and susceptibility to contraction-induced injury (29, 30, 33). Here we report that similar results were achievable in the *mdx:utr*^{-/-} mouse with TAT- μ Utr and likely contribute to improvements in ambulation.

The culmination of increased muscle function, animal mobility, and food consumption in the *mdx:utr*^{-/-} mouse appeared to be manifested by extended life span. Previous reports on *mdx:utr*^{-/-} mouse life span is highly variable, ranging from as little as 4 wk to as many as 36 wk (5, 8, 10, 13, 15, 17, 24). This variability may reflect genetic drift within respective colonies and local environmental factors idiosyncratic to each housing facility (e.g., staff, cage sizes, husbandry, handling, food enrichment options, room noise, architecture, temperature, etc.). While these variables may confound the external validity of certain findings and make inter-laboratory compar-

isons difficult, it is important to consider these types of various contributing factors. Here, we measured life spans of 7 and 9 wk for *mdx:utr*^{-/-} mice treated with PBS and TAT- μ Utr, respectively, and two factors may have contributed to the relatively short life spans. First, we individually housed each *mdx:utr*^{-/-} mouse during the life span analysis to ensure consistency of housing from litter to litter. The low body mass and activity of *mdx:utr*^{-/-} mice impeded the conservation of heat, and individually housed animals were frequently observed shivering. Second, all mice in the study endured twice weekly handling required for IP injections, which likely added stress. Nonetheless, both PBS and TAT- μ Utr mice were handled identically and we observed an improvement in life span of the mice that received TAT- μ Utr treatments.

Loss of muscle function is a well-established consequence of dystrophin deficiency (4, 7, 8, 13). Herein, we observed modest, but significant improvements in skeletal muscle function and life span of TAT- μ Utr mice. We conclude TAT- μ Utr may be a viable treatment strategy for patients with DMD; however, investigation into its effectiveness in combination with other therapies as well as its effects on muscle recovery and adaptation are warranted.

GRANTS

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DISCLOSURES

J. M. Ervasti is a coinventor on US Patent No. 7,863,017: TAT-Utrophin as a Protein Therapy for Dystrophinopathies.

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